Effects of the leak conductance in the synchronization of a Hodgkin-Huxley type network.

Perspectives on Oscillation Control

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Abstract In this work, we studied how the distinction of the leak conductance in the Huber and Braun *et al.* model affects the synchronization of a neuronal network. We simulated the distinction of the parameter using a truncated gaussian distribution, following the dynamical limits of the conductance.

Introduction

Results

In this work, we numerically simulated the synchronization of a small-world network with N = 512 neurons. First, we calculated the bifurcation diagram of the interspike interval (*ISI*) so we can understand what is the dynamics of the leak conductance (Figure 2). We observed that for values greater than $\bar{g}_L = 0.15$ there is no bursting or spike regime, so for our parameter space analysis, we limited the distributions to values of $0.06 \leq \bar{g}_L \leq 0.15$. In Figure 3 we simulated truncated gaussian distributions, where σ is the standard deviation, to several values of the leak conductance and observed the synchronization pattern of the network when we forced the coupling parameter.

1st Perspectives on Oscillation Control

In 1952 Alan Lloyd Hodgkin and Andrew Huxley proposed a mathematical model for the action potential of a neuron [1], which later awarded them with the Nobel Prize in Phisiology. The main equation is:

$$C_M \frac{\mathrm{d}V}{\mathrm{d}t} = -I_K - I_{Na} - I_L + I_{ext}.$$

The equation comes from the capacitor equation, with C_M being the membrane capacitance, V is the associated potential, and I_K , I_{Na} , I_L and I_{ext} are, the current associated with the potassium ion, the sodium ion, the leak current and an external current, respectively. The currents can be written as

$$I_K = \bar{g}_K n^4 (V - E_K),$$

$$I_{Na} = \bar{g}_{Na} m^3 h (V - E_{Na}),$$

$$I_L = \bar{g}_L (V - E_L),$$

where \bar{g}_K , \bar{g}_{Na} and \bar{g}_L are the associated conductancies, and E_K , E_{Na} , E_L represents the rest potential from each ion. The parameters m, n and h are experimentally obtained.

The Huber-Braun equations

The Hodgkin-Huxley model is not capable to reproduce the bursting of spikes dynamics of a neuron, so Huber and Braun *et al.* [2] modelled the equations to be thermally sensitive, with addition of two currents, I_{sd} and I_{sa} , that are responsible for the activation when the potential is bellow a threshold. The new set of equations are:

$$C_M \frac{\mathrm{d}V}{\mathrm{d}t} = -I_K - I_{Na} - I_{sd} - I_{sa} - I_L + I_{ext},$$

and the new currents with temperature dependence:

$$I_{K} = \rho \bar{g}_{K} a_{K} (V - E_{K}),$$

$$I_{Na} = \rho \bar{g}_{Na} a_{Na} (V - E_{Na}),$$

$$I_{sd} = \rho \bar{g}_{sd} a_{sd} (V - E_{sd}),$$

$$I_{sa} = \rho \bar{g}_{sa} a_{sa} (V - E_{sa}),$$

$$I_{L} = \bar{g}_{L} (V - E_{L}),$$



Figure 2: Bifurcation diagram of the interspike interval for a Poincaré surface at -20 mV.



where a_K , a_{Na} , a_{sd} , a_{sa} , are ionic channels opening probabilities and ρ is a function with temperature dependence.

In a network with N neurons, coupled with a Small-World adjacency matrix, the Huber-Braun equations to the *i*-th neuron, is

$$C_M \frac{\mathrm{d}V^{(i)}}{\mathrm{d}t} = -I_K^{(i)} - I_{Na}^{(i)} - I_{sd}^{(i)} - I_{sa}^{(i)} - I_L^{(i)} + I_{coup}^{(i)},$$

with

$$I_{coup}^{(i)} = \frac{\epsilon}{n} \sum_{j=1}^{N} e_{(ij)} r^{(j)} (V_{sin} - V^{(i)}),$$

the $e_{(ij)}$ are the adjacency matrix elements, ϵ is the coupling parameter, V_{sin} is a sinaptic potential, n is the normalization from the most connected neuron and $r^{(j)}$ is a differential equation that simulates the channel opening. In Figure 1 we can see how the coupling parameter may affect the bursting of neurons.





Figure 3: Parameter space for different values of standard deviation of the gaussian distribution for the leak conductance. With $\sigma = 0.00$ a network when the conductance is fixed.

Figure 1: Bursting neurons regime with (a) $\epsilon = 0.0$ and (b) $\epsilon = 0.08$.

Phase synchronization

A phase $\theta^{(j)}(t)$ can be associated with the *j*-th bursting neuron with t as the time of integration, $t_k^{(j)}$ as the time of the *k*-th neuronal spike and $t_{k+1}^{(j)}$ as the following spike.

$\theta^{(j)}(t) = 2\pi k^{(j)} + 2\pi \frac{t - t_k^{(j)}}{t_{k+1}^{(j)} - t_k^{(j)}},$

The Kuramoto order parameter [3] can be associated with this phase

$$z(t) = R(t)e^{i\psi(t)} = \frac{1}{N}\sum_{j=1}^{N} e^{i\theta^{(j)}(t)},$$

where R(t) is the modulus of z(t) and N is the number of oscillators. The temporal average of the parameter can be obtained with

$\langle R \rangle = \frac{1}{t_f - t_i} \sum_{t=t_i}^{t_f} R(t).$

Conclusions

A small distinction of the leak conductance, such as $\sigma = 0.001$, may not affect values bigger than $\epsilon = 0.03$ of the coupling strength, but it can affect lower values. However, for $\sigma = 0.01$, it affects the network as a whole, slowering the synchronization process and eliminating all of the synchronized regions with lower values of ϵ .

References

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Acknowledgements

